

^{18}F -Labeling and evaluation of novel MDL 100907 derivatives as potential 5-HT_{2A} antagonists for molecular imaging

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Abstract

Introduction: The serotonergic system, especially the 5-HT_{2A} receptor, is involved in various diseases and conditions. It is a very interesting target for medicinal applications.

Methods: Two novel 5-HT_{2A} tracers, namely, [^{18}F]DD-1 and the enantiomeric pure (*R*)-[^{18}F]MH.MZ, were radiolabeled by ^{18}F -fluoroalkylation of the corresponding desmethyl analogue. In vitro binding autoradiography on rat brain slices was performed to test the affinity and selectivity of these tracers. Moreover, first μPET experiments of (*R*)-[^{18}F]MH.MZ were carried out in Sprague-Dawley rats.

Results: [^{18}F]DD-1 ($K_i=3.23$ nM) and (*R*)-[^{18}F]MH.MZ ($K_i=0.72$ nM) were ^{18}F -fluoroalkylated by the secondary synthon [^{18}F]FETos in a radiochemical yield (RCY) of >70%. The final formulation for both tracers took no longer than 100 min with an overall RCY of ~40%. It provided [^{18}F]tracers with a purity >96% and a typical specific activity of 25–35 GBq/ μmol . Autoradiographic images of (*R*)-[^{18}F]MH.MZ (**5**) and [^{18}F]DD-1 (**4**) showed excellent visualization and selectivity of the 5-HT_{2A} receptor for (*R*)-[^{18}F]MH.MZ and less specific binding for [^{18}F]DD-1. The binding potential (BP) of (*R*)-[^{18}F]MH.MZ was determined to be 2.6 in the frontal cortex and 2.2 in the cortex ($n=4$), whereas the cortex-to-cerebellum ratio was determined to be 3.2 at steady state ($n=4$). Cortex-to-cerebellum ratios of (*R*)-[^{18}F]MH.MZ were almost twice as much as compared with the racemic [^{18}F]MH.MZ. Thereby, equal levels of specific activities were used. High uptake could be demonstrated in cortex regions.

Conclusion: Labeling of both novel tracers was carried out in high RCY. Autoradiography revealed (*R*)-[^{18}F]MH.MZ as a very selective and affine 5-HT_{2A} tracer ($K_i=0.72$ nM), whereas [^{18}F]DD-1 showed no reasonable distribution pattern on autoradiographic sections. Moreover, results from μPET scans of (*R*)-[^{18}F]MH.MZ hint on improved molecular imaging characteristics compared with those of [^{18}F]MH.MZ. Therefore, (*R*)-[^{18}F]MH.MZ appears to be a highly potent and selective serotonergic PET ligand in small animals.

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Keywords: MDL 100907; MH.MZ; PET; Fluorine-18; 5-HT_{2A} receptor

1. Introduction

Several diseases and physiological processes, including appetite, emotion, changes in mood, depression, Alzheimer's disease and the regulation of the sleep/wake cycle, are involved in the serotonergic system [1–3]. In particular, many clinically approved atypical antipsychotic drugs are

potent 5-HT_{2A} receptors [4]. Therefore, in vivo positron emission tomography (PET) studies of the 5-HT_{2A} receptor occupancy and availability would provide a significant advance in the understanding of the mentioned disorders and conditions. PET is an appropriate tool to measure noninvasively and repetitively various parameters like the binding potential, the receptor availability and uptake kinetics of radiotracers for neuroreceptors in vivo. Novel ^{18}F -labeled 5-HT_{2A} antagonists would provide a significant advance in the field of molecular imaging of the serotonergic system as clinically used ligands to study the 5-HT_{2A} receptor, like [^{18}F]altanserin or [^{11}C]MDL 100907, have notable disadvan-

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tages. [^{11}C]MDL 100907 is a very specific high-affinity ligand for 5-HT $_2\text{A}$ receptors with limitations due to its slow kinetics and the short half-life of C-11 [5–7]. The binding of [^{18}F]altanserin lacks specificity and in vivo stability [8,9].

Recently, we have reported the syntheses and first in vitro and in vivo evaluation of [^{18}F]MH.MZ (1), an ^{18}F -analog of MDL 100907 (Fig. 1) [9,10]. The novel labeling reaction route could possibly be a superior one compared to that of [^{18}F]altanserin. In vivo and in vitro studies defined [^{18}F]MH.MZ as a potent tracer to image the 5-HT $_2\text{A}$ receptor status via PET at least in rats [10].

With these encouraging results, a new series of MDL 100907 derivatives were synthesized aiming for even more selective reference ligands [11].

Due to experiments carried out in vitro, two novel and potent compounds [DD-1 and (*R*)-MH.MZ], displayed in Fig. 2, showed promising characteristics as high-affinity and selectivity ligands (Fig. 2) [11].

These results justified further experiments like in vitro autoradiography and in vivo microPET (μPET) experiments to prove the applicability of these two novel ligands. The manuscript reports on the labeling of DD-1 and (*R*)-MH.MZ with F-18 and their evaluation as potential new and improved 5-HT $_2\text{A}$ imaging agents in rats.

2. Methods and materials

2.1. Chemicals and reagents

All reagents and solvents used were of analytical-grade quality and purchased from Acros, Fluka or Merck. Unless otherwise noted, all chemicals were used without further purification.

2.2. High-performance liquid chromatography

2.2.1. Analytical HPLC

A high-performance liquid chromatography (HPLC) system was used equipped with a Sykam S 1100 solvent delivery system, S 8110 low pressure gradient mixer, Rheodyne 9725i inject valve; linear UVIS-205 absorbance detector; Axxiom Chromatography 900-200 Pyramid; Pyramid 2.07; loop: 20 μl .

2.2.2. Semipreparative HPLC

A HPLC system equipped with a Dionex P680A pump, a Raytest NaI scintillation counter (Gabi) and a Dionex UVD 170U (254 nm) absorbance detector was used.

Dionex Chromeleon software was used for UV-data analysis and Raytest Gina-star software was used for radioactivity detection.

2.3. Hardware

2.3.1. Imager

Autoradiographic images were analyzed via an image analyzer (FLA 7000 Fujifilm). Radioactive spots were detected using a Canberra Packard Instant Imager.

2.3.2. MicroPET

PET studies were performed with a Siemens MicroPET Focus 120 camera.

2.4. Animals

Male, 8-week-old, mature catheterized Sprague-Dawley (SD) rats obtained from the animal husbandry of the Johannes Gutenberg University of Mainz, Germany, were used for ex vivo distribution as well as for PET studies. All procedures were carried out in accordance with the European Communities Council Directive regarding care and use of animals for experimental procedures and were approved by local authorities of the state of Rhineland-Palatine.

2.5. Preparation of rat brain sections

Rats were narcotized with CO $_2$ and subsequently decapitated by a rodent guillotine. Brains were carefully removed from the skull and shortly rinsed in ice-cold 50 mM Tris/citrate (pH 7.4) buffer to remove hairs and blood. The brains were then frozen on a precooled -80°C cold steel plate. Brains were either stored in parafilm or in aluminum foil at -80°C or transferred to a Leica cryostat and kept in parafilm at -24°C for 30 min. After warming up to -24°C , brains were frozen onto an object carrier with tissue tack freezing medium in the desired orientation for either sagittal, coronal or transversal sectioning. Sections were cut at 14 μm thickness, knife angle of 5° and an object temperature of -13°C . Sections were melted onto super frosted glass slides (Menzel), air dried and were either used immediately or stored at -80°C until further use.

2.6. Radiochemistry

2.6.1. Preparation of the $K[^{18}\text{F}]F-K_{222}$ complex

An anion exchange resin (Sep-Pak Light Waters Accell Plus QMA cartridge) was washed with aqueous 1 M K $_2\text{CO}_3$ (10 ml) and rinsed with water (20 ml) and CH $_3\text{CN}$ (10 ml) by

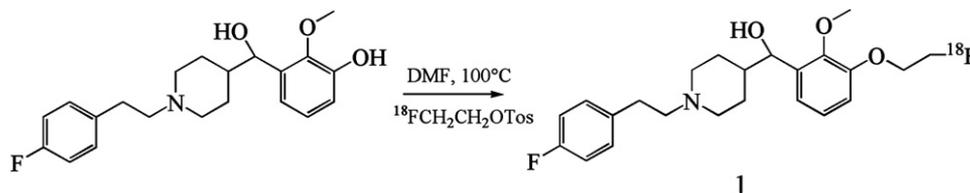


Fig. 1. Radiosynthesis of [^{18}F]MH.MZ.

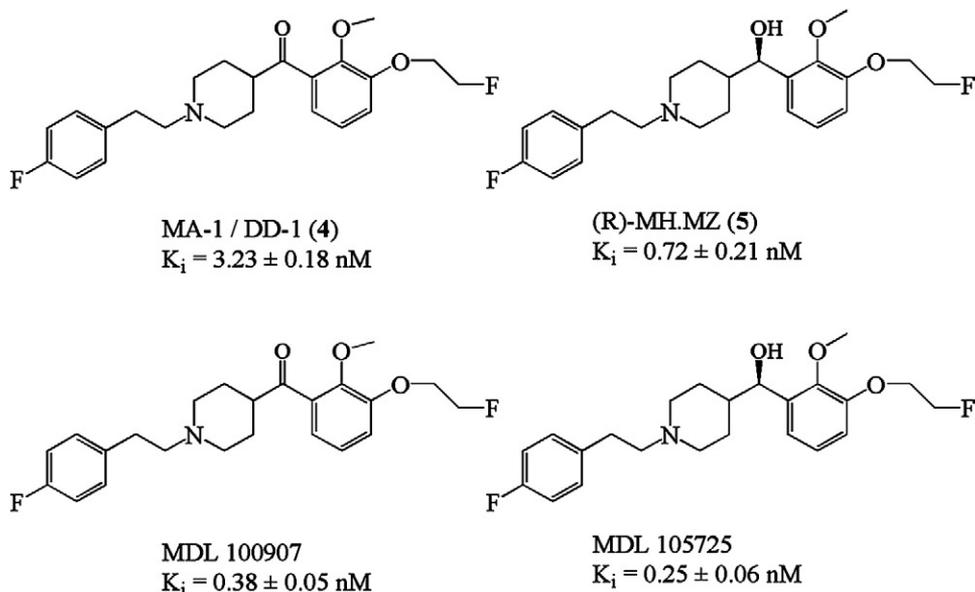


Fig. 2. Structures of new potent, selective [18 F]ligands of the 5-HT_{2A} receptor, the original 11 C-labeled compound and its precursor MDL 105725 [11].

helium pressure (1.5–2 bar). Then the aqueous [18 F]fluoride solution was passed through this exchange resin. [18 F]Fluoride ions were then eluted from the resin using 15 μ l of 1 M K₂CO₃ solution and 15 mg Kryptofix₂₂₂ (K₂₂₂: 4,7,13,16,21,24-hexaoxa-1,10diazabicyclo[8.8.8]hexacosane). The resulting solution was then gently concentrated to dryness at 90°C under a nitrogen stream for 15 min to give no-carrier-added K[18 F]F–K₂₂₂ complex as a white semi-solid residue.

2.6.2. Radiosynthesis of [18 F]FETos

The dried K[18 F]F–K₂₂₂ complex was then dissolved in 1 ml acetonitrile, and 4 mg (10 mmol) ethylenglycol-1,2-ditosylate was added and heated under stirring in a sealed vial for 3 min. Purification of the crude product was accomplished using HPLC (Lichrospher RP18-EC5; 250×10 mm; acetonitrile/water 50:50; flow rate: 5 ml/min; retention time [RT]: 8 min). After diluting the HPLC fraction containing the 2-[18 F]fluoroethyltosylate with water, the product was loaded on a Phenomenex strata-X 33- μ m polymeric reversed-phase column, dried with nitrogen and eluted with 1 ml of tempered (40–50°C) DMSO.

2.6.3. General procedure of the synthesis of [18 F]FE-MDL 100907 derivatives

[18 F]FETos trapped on a Phenomenex strata-X 33- μ m polymeric reversed-phase column was directly rinsed with 1 ml of tempered (40–50°C) DMSO into a vial with 3 mg precursor (8.3 μ mol) and 1.5 μ l 5N NaOH (7.5 μ mol). The tube was placed in a heating block and stirred during the reaction time. The reaction vessel was then cooled to room temperature using an ice-water bath and quenched with 1 ml H₂O. The remaining radioactivity was measured, which was 90–95% of the initial radioactivity. The resulting reaction

mixture was analyzed by radio-TLC. The reaction yield was calculated from the TLC-radiochromatogram and defined as the ratio of radioactivity area of the 18 F-labeled compound over total fluorine-18.

(R)-[18 F]MHMZ: SiO₂-TLC, eluent: CHCl₃/MeOH/conz. NH₃, 8:1:0.2; (R)-[18 F]MHMZ: R_f =0.36, [18 F]FETos: R_f =0.95, [18 F]fluoride ion: R_f =0.0.

[18 F]DD-1: SiO₂-TLC: eluent: CHCl₃/MeOH, 20:1; [18 F]DD-1: R_f =0.72; [18 F]FETos: R_f =0.97; [18 F]fluoride ion: R_f =0.0.

2.6.4. Formulation

Formulation of the labeled product for evaluation studies was effected as follows: reactants and byproducts were separated from 18 F-tracers by semipreparative HPLC (μ Bondapak C₁₈ 7.8×300 mm column; RT; flow rate 8 ml/min).

(R)-[18 F]MHMZ: 0.05 M Na₂HPO₄ (pH 7.4 H₃PO₄)/MeCN, 60:40 RT; [18 F]F[−]=1.8 min; [18 F]FETos=4 min; (R)-[18 F]MHMZ=9.76 min; MDL 105725 (2)=4.85 min. [18 F]DD-1: 0.25 M NH₄Ac buffer (pH 5.6 acetic acid)/MeCN, 75:25; RT: [18 F]F[−]=2.5 min; [18 F]FETos=11.54 min; [18 F]DD-1=21.73 min; [precursor (3)]=7.23 min.

The collected fraction containing the 18 F-labeled compound with water (4:1) was passed through a conditioned strataX-cartridge (1 ml EtOH, 1 ml H₂O) and washed with 10 ml H₂O. The 18 F-labeled compound was eluted with at least 1 ml of EtOH. Less than 8% of the total radioactivity was left on the cartridge. Finally, EtOH was removed in vacuo and the 18 F-labeled tracer was solved in 1 ml saline.

2.6.5. Quality control

The radiotracer preparation was visually inspected for clarity, absence of color and particulates. Chemical and radiochemical purities were also assessed on an aliquot by TLC analyses and by analytical HPLC (ET 250/8/4 Nucleosil 5 C₁₈). (R)-[¹⁸F]MHMZ: see above.

[¹⁸F]DD-1: NH₄Ac buffer (pH 5.6)/MeCN, 60:40; flow rate 1 ml/min; RT: [¹⁸F]F⁻=2.4 min; [¹⁸F]FETos=16.34 min; [¹⁸F]DD-1=24.63 min; [precursor (3)]=11.40.

Specific activity (*A_s*) of the radiotracer was calculated from three consecutive HPLC analyses (average) and determined as follows: the area of the UV absorbance peak of the ¹⁸F-analogue of the ¹⁸F-labeled tracer was integrated on the HPLC chromatogram and compared to a standard curve relating mass to UV absorbance.

2.7. In vitro autoradiography of rat brain slices with [¹⁸F]DD-1 and (R)-[¹⁸F]MH.MZ

Autoradiography experiments were carried out at room temperature in reaction buffer (50 mM Tris/HCl buffer, pH 7.4, containing 120 mM NaCl and 5 mM KCl) with ¹⁸F-labeled compounds on ice. In the case of the challenge experiments (Section 3.2; Fig. 6), four competitors, ketanserin, fallypride, WAY 100635 and prazosin, were added in excess (10 μM).

Sections were washed 2×2 min in reaction buffer containing 0.01% Triton X-100 and 1×2 min in reaction buffer, shortly dipped into deionized water and quickly dried in a stream of cold air. Sections were exposed to Fuji phosphor screen for 3 h. Screens were read out with a Fuji FLA-7000 scanner. ¹⁸F-Quantification was done after calibration by a standard curve which was obtained by a dilution series of an ¹⁸F-solution. Calibration was repeated for each fresh radiotracer synthesis. Calibration, quantification and data evaluation were done with the Fujifilm MultiGauge image analysis software.

2.8. In vivo PET studies of (R)-[¹⁸F]MH.MZ

Positron emission tomography scans were performed with a Siemens/Concorde Microsystems microPET Focus 120 small animal PET (μPET) scanner. Eight-week-old male Sprague-Dawley rats (weight: 220–325 g) were obtained from the animal husbandry of the Johannes Gutenberg University of Mainz. Animals were anesthetized with a combination of xylazine (Rompun) (2%) and ketamine (Ketavet) (10%) by intraperitoneal injection of 1.1 ml/kg. Rats were placed in supine position on the scanner bed and fixed with adhesive strips. Listmode acquisition was started with the tracer injection of 15 MBq (specific activity: 35–45 GBq/μmol). The ¹⁸F-labeled tracer was applied via intravenous injection into the femoral vein catheter. Then, catheters were flushed with 0.25 ml isotonic 0.9% NaCl solution.

After the dynamic recordings, a transmission scan for attenuation correction was carried out using a ⁵⁷Co point source. Listmode acquisition was histogrammed into 25 frames. The frame duration increased progressively from 20 s to 5 min resulting in a total scanning time of 90 min. Finally, images were reconstructed with scatter and attenuation correction using a 3D maximum a posteriori (MAP) algorithm with 18 iterations and regularization parameter of 0.002.

Images were scaled as standardized uptake values (SUVs) which is defined as: activity concentration in becquerel per milliliter×body weight in grams/injected dose in becquerel. Kinetic modeling and image quantification were carried out using the PMOD software package. First, the images were transformed into standardized views according to the Paxinos orientation. A volume-of-interest (VOI) template comprising the frontal cortex, cortex [motor and somatosensory cortex (parietal and temporal cortex)] and the cerebellum was defined on transaxial slices using an integral image between 60 and 90 min postinjection reflecting specific binding of the tracer. Time–activity curves (TAC) were derived from dynamic kinetics. Assuming negligible receptor density, the cerebellum was used as a reference region. Binding potential (BP) was calculated using the TAC and the simplified reference tissue model.

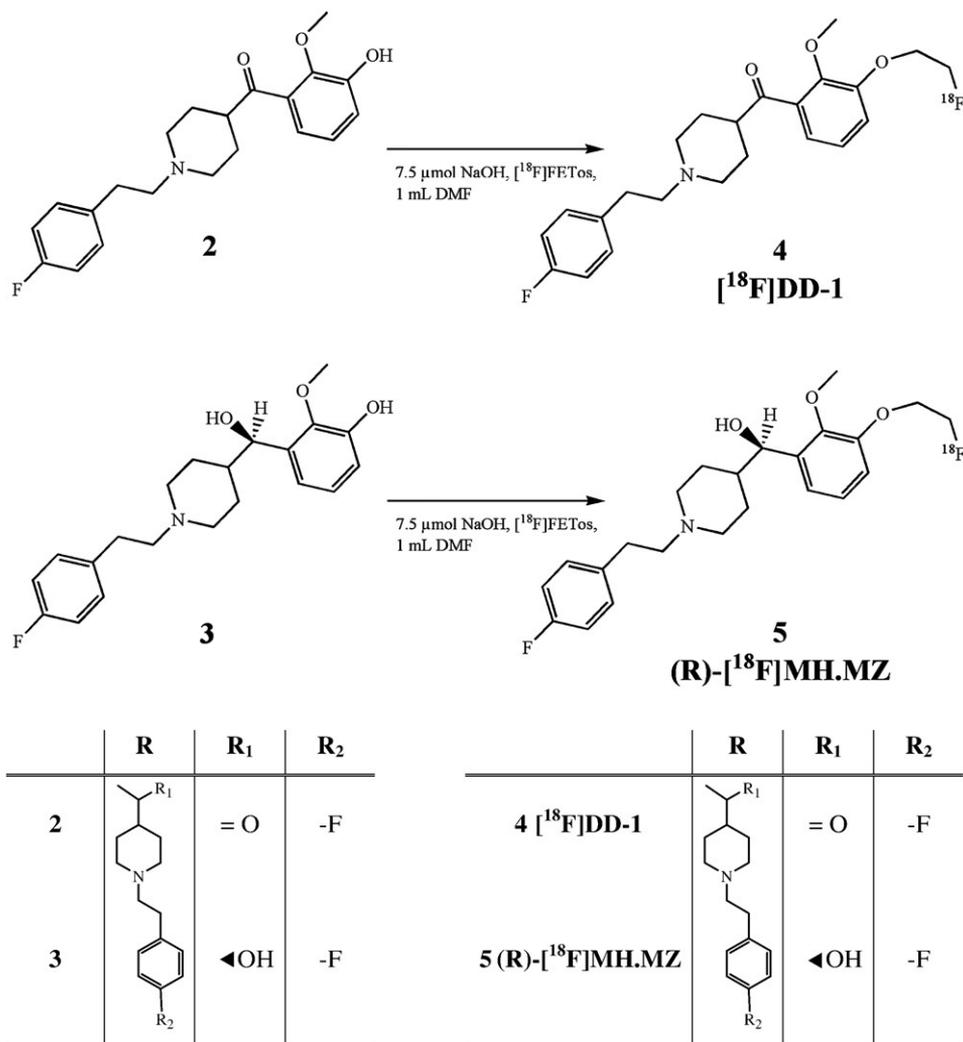
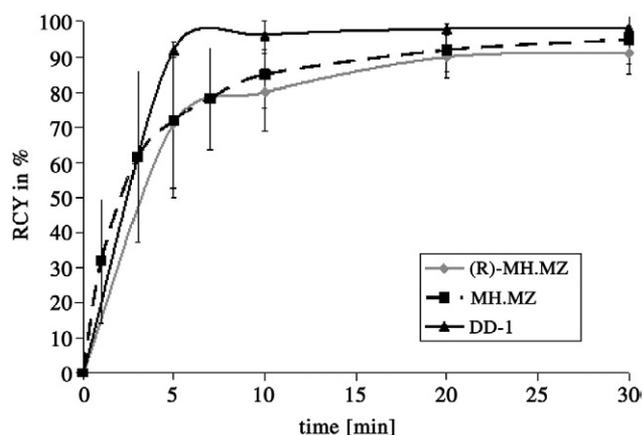
3. Results and discussion

3.1. Radiochemistry

Precursors and reference compounds were synthesized as previously described [11]. Radioactive labeling was carried out similar to the reported synthesis of [¹⁸F]MH.MZ [9,10]. Thereby, necessary [¹⁸F]FETos synthon production was performed in an automated module according to Bauman et al. [12] and used for [¹⁸F]fluoroalkylation resulting in (R)-[¹⁸F]MH.MZ and [¹⁸F]DD-1 (Fig. 3).

[¹⁸F]Fluoroalkylation of the precursor (2) was optimized only due to temperature variations resulting in radiochemical yields >70%. Labeling kinetics were compared with those reported for [¹⁸F]MH.MZ, whereas the [¹⁸F]alkylation of the enantioselective precursor (R)-MDL 105725 (3) was carried out using exactly the same reaction conditions as for its racemic analog. Used parameters enable radiochemical yields of about 80%. Final reaction conditions were 100°C, 15 min reaction time, 7 mmol precursor, 7 mmol 5N NaOH and dry DMSO (Fig. 4).

The final formulation of the injectable solution including a semipreparative HPLC took no longer than 100 min for all compounds and provided ¹⁸F-labeled tracers with a radiochemical purity of >96% and a chemical purity of >98% indicated by HPLC analyses. Typical specific activities (*A_s*) are between 35 and 45 GBq/μmol. Thereby, amounts of ~3 GBq of [¹⁸F]fluorine were used as starting radioactivity.

Fig. 3. Syntheses of [¹⁸F]DD-1 and (R)-[¹⁸F]MH.MZ.Fig. 4. ¹⁸F-Fluoroalkylation of 7 mmol precursor at 100°C using DMF and 7 mmol 5N NaOH yielding [¹⁸F]MH.MZ, [¹⁸F]DD-1 and (R)-[¹⁸F]MH.MZ.

The new ¹⁸F-labeled compounds could be obtained as an injectable solution in an overall radiochemical yield of about 40% referred to the starting activity of ¹⁸F-fluoride. This is very similar to the radiosynthesis of [¹⁸F]altanserin, which takes 75 to 100 min and results in a radiochemical yield of 30–50% [13].

3.2. In vitro autoradiography

Autoradiographic images obtained with (R)-[¹⁸F]MH.MZ (5) and [¹⁸F]DD-1 (4) showed accumulation of radioactivity in known 5-HT_{2A} receptor regions in rat brain slices at equal A_s of 30 GBq/μmol (Fig. 5).

Excellent visualization was obtained by (R)-[¹⁸F]MH.MZ. These data are in accordance with the known distribution of [³H]MDL 100907 [14,15] and [¹⁸F]MH.MZ [9] in the rat brain.

Due to the higher 5-HT_{2A} binding of (R)-MH.MZ (K_i=0.72 nM) compared to MH.MZ (K_i=3.0 nM), this enantioselective tracer should be more valuable in PET experiments concerning the possibly improved binding

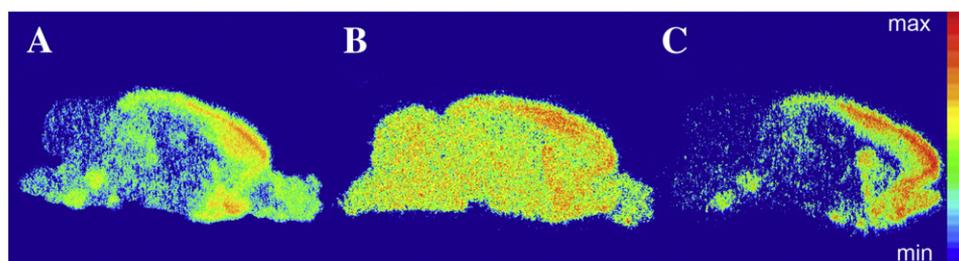


Fig. 5. Images of an autoradiography of [^{18}F]MH.MZ (left), (R)-[^{18}F]MH.MZ (right) and [^{18}F]DD-1 (middle) show high specific binding for the MH.MZ analogues and less for [^{18}F]DD-1 at 14- μm -thick rat brain sections; major binding was detected in lamina V of the frontal cortex.

potential (BP) and the regional cortex-to-cerebellum ratio within the brain.

Visualization by [^{18}F]DD-1 showed less specific binding (Fig. 5). Indeed, reduced binding characteristics could be expected due to its decreased affinity compared to (R)-[^{18}F]MH.MZ (Table 1), but were not necessarily likely for [^{18}F]DD-1 compared to its [^{18}F]MH.MZ analogue (Table 1). In addition, selectivity of [^{18}F]DD-1 showed no intense alteration compared to that of MH.MZ [11]. Therefore, the observed properties are most probably due to the increased lipophilicity of [^{18}F]DD-1 (MH.MZ: $\log P=2.80\pm 0.06$; DD-1: $\log P=3.08\pm 0.1$) [11].

Competition autoradiography experiments (Fig. 6) were conducted with the new enantioselective tracer to prove its potential as a PET imaging agent. Thereby, 1 nM of (R)-[^{18}F]MH.MZ and 10 μM of ketanserin, fallypride, WAY 100635 and prazosin were used in these competition assays. High specificity of (R)-[^{18}F]MH.MZ toward the 5-HT $_{2A}$ receptors was obtained as expected because of the affinity and selectivity determined by radioligand binding assays through the NIMH Psychoactive Drug Screening Program (PDSP) [11].

Total displacement could be observed with ketanserin as a known 5-HT $_{2A}$ receptor ligand, whereas no displacement could be detected with WAY 100635, a 5-HT $_{1A}$ antagonist, and prazosin, an α_1 ligand. Another displacement could only be detected with fallypride. However, co-incubation of fallypride led to a displacement of $25\pm 8\%$ ($n=4$) of total binding in the frontal cortex as well as in the caudate-putamen, which does not imply that [^{18}F]MH.MZ recognizes D $_2$ /D $_3$ receptors but might rather be explained by the known cross affinity of fallypride to 5-HT $_2$ receptors (Fig. 6) [16]. These results are very similar to those observed with

the racemic analogue, [^{18}F]MH.MZ [9] and [^3H]MDL 100907 [14,17]. Especially, the advantage of MDL 100907 over altanserin regarding the D $_2$ affinity could be retained by both the racemic and its enantioselective ligand (R)-[^{18}F]MH.MZ. Herth et al. [9] demonstrated this superior in vitro behavior of [^{18}F]MH.MZ by autoradiographic experiments. Whereas [^{18}F]altanserin showed a strong D $_2$ binding within the striatum, no specific accumulation could be observed either by [^{18}F]MH.MZ [9] or by (R)-[^{18}F]MH.MZ (Fig. 5) in these regions.

Binding parameters of (R)-[^{18}F]MH.MZ of cortex-to-cerebellum ratios of the rat brain obtained with autoradiography assays at equal levels of specific activities at sagittal sections are shown in Table 1 and compared with the binding parameters of [^{18}F]MH.MZ and [^3H]MDL 100907 [9]. Binding in the cerebellum was at the level of nonspecific binding, so levels of binding in different brain regions are also given relative to that brain area. However, as a matter of fact, (R)-[^{18}F]MH.MZ showed region-to-cerebellum ratios almost twice as high as compared with [^{18}F]MH.MZ. Results of [^{18}F]DD-1 were not evaluated due to its unfavorable distribution pattern.

In conclusion, the results suggest that the nonspecific binding associated with these radiotracers is low for [^{18}F]MH.MZ and (R)-[^{18}F]MH.MZ and moderate to low for [^{18}F]DD-1 (Fig. 4). [^{18}F]MH.MZ and (R)-[^{18}F]MH.MZ could possibly be useful as ^{18}F -labeled tracers for imaging the 5-HT $_{2A}$ receptor in vivo by PET experiments. Especially, (R)-[^{18}F]MH.MZ could improve binding characteristics such as BP or regional distribution expressed as cortex-to-cerebellum ratios due to its higher affinity. In comparison to [^3H]MDL 100907 and [^{18}F]altanserin, (R)-[^{18}F]MH.MZ and also [^{18}F]MH.MZ are in no way inferior in terms of specificity for 5-HT $_{2A}$ receptors and region cortex-to-cerebellum ratios [9,14,17].

Table 1

Binding parameters obtained with (R)-[^{18}F]MH.MZ and [^{18}F]MH.MZ from binding in vitro autoradiographic experiments at 14- μm -thick sagittal sections of the rat brain

	<i>n</i>	(R)-[^{18}F]MH.MZ	[^{18}F]MH.MZ	[^3H]MDL 100907
		Region/cerebellum ratio		
Lamina V	4	91.8 \pm 0.5	59.5 \pm 2.8	105.5 \pm 0.8
Frontal cortex	4	57.5 \pm 3.2	31.4 \pm 1.3	54.4 \pm 4.2

Values are shown as means \pm S.E.M.

3.3. In vivo PET experiments

Due to the relatively moderate binding characteristics of [^{18}F]DD-1, only PET scans with (R)-[^{18}F]MH.MZ were performed, expecting better in vivo results compared to with its racemic derivative [^{18}F]MH.MZ. Dynamic images were analyzed with pixel-wise modeling computer software (PMOD; Zurich, Switzerland). For illustrative purposes,

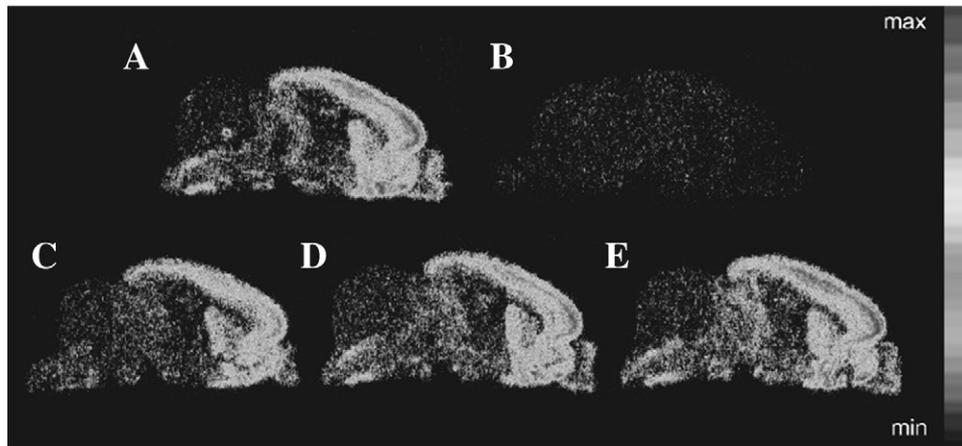


Fig. 6. Sagittal autoradiographies on 14- μ m-thick rat brain sections with (*R*)-[18 F]MHMZ at a concentration of 1 nM ($K_i=0.72$ nM for 5-HT $_{2A}$). (A) Total binding, (B) nonspecific binding measured in the presence of 10 μ M ketanserin, (C) co-incubation with 10 μ M fallypride, (D) co-incubation with 10 μ M WAY 100635, (E) co-incubation with 10 μ M prazosin.

an integral image between 60 and 90 min after tracer injection is displayed in Fig. 7, whereby the last 30 min of the dynamics reflects the specific binding of (*R*)-[18 F]MH.MZ. Images are shown in horizontal orientation with a slice thickness of 0.8 cm. False color-coded images in Fig. 7A display horizontal slices through the rat brain from top (1) to bottom (12), whereas Fig. 7B shows a representative horizontal slice through the cortex, the frontal cortex and the cerebellum area.

These PET images clearly visualize the binding of (*R*)-[18 F]MH.MZ in the frontal cortex known to possess high availability of 5-HT $_{2A}$ receptors, whereas the cerebellum,

which is believed to be devoid of 5-HT $_{2A}$ receptors, is at background level [14]. Results are very similar to those obtained by its racemic analogue [18 F]MH.MZ.[9]

Fig. 8 shows a representative time–activity curve (TAC) of a total binding study of (*R*)-[18 F]MH.MZ which included four animals. Results are given as standardized uptake value (SUV) (% injected dose in becquerel per milliliter \times animal weight in grams). Uptake of (*R*)-[18 F]MH.MZ between 60 and 90 min is more than 150% higher in cortical regions than in the cerebellum, whereas the uptake of [18 F]MH.MZ is only 50% higher in these regions [9]. The binding potential (BP) of (*R*)-[18 F]MH.MZ was determined to be 2.6 for the

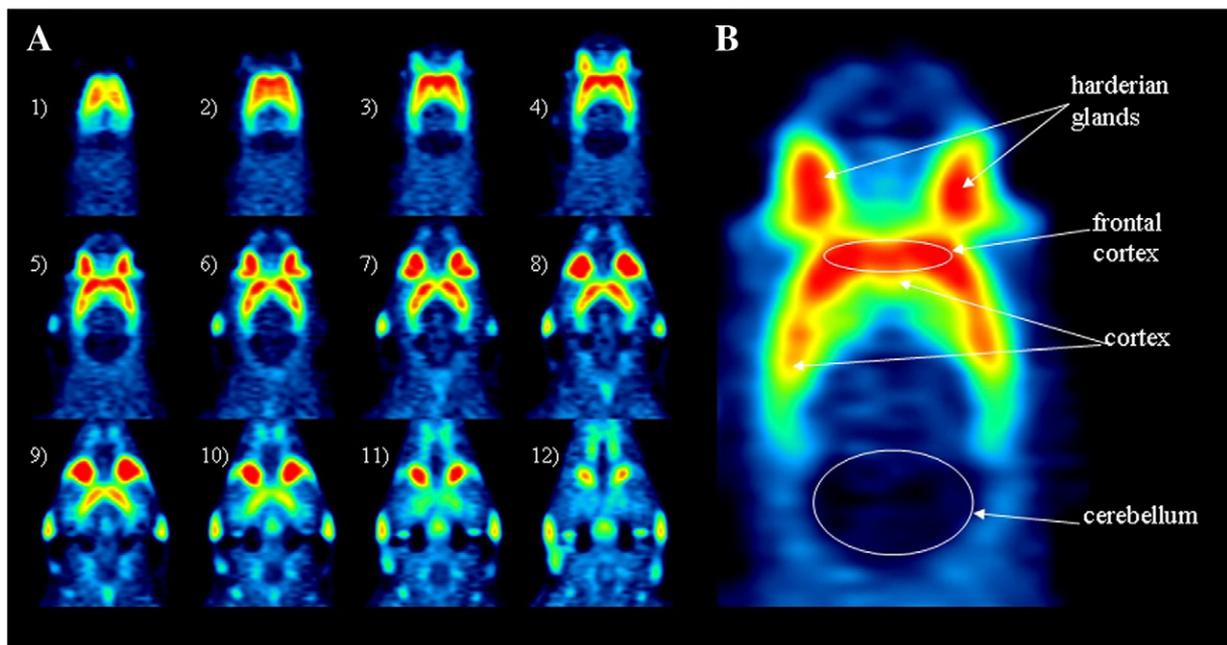


Fig. 7. MicroPET images of (*R*)-[18 F]MH.MZ binding in horizontal orientation. (A) Horizontal slices from top (1) to bottom (12). (B) Representative horizontal slice through the cortex, the frontal cortex and the cerebellum showing highest specific binding in the frontal cortex and a high nonspecific binding in the harderian glands. Uptake in the cerebellum was at background level.

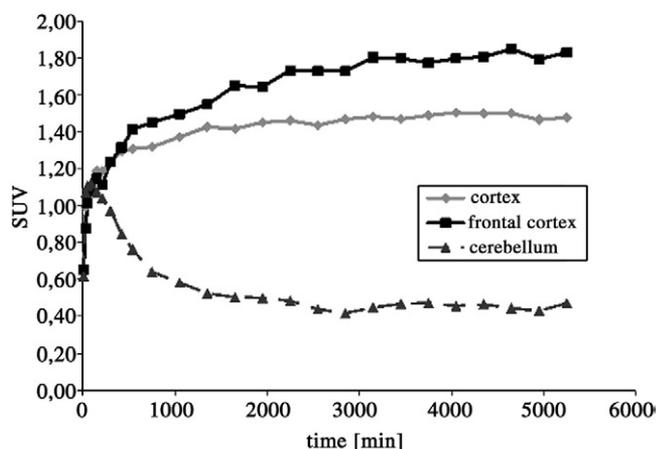


Fig. 8. Representative time–activity curve (TAC) of μ PET experiments of (R)-[^{18}F]MH.MZ in SD rats. The graph shows the results of a total binding study. Results are given as SUV (% injected dose in becquerel per milliliter \times animal weight in grams).

frontal cortex region and to be 2.2 for the cortex ($n=4$) using a simplified reference tissue model and the PMOD software, whereas the BP for its racemic derivative, [^{18}F]MH.MZ, was only determined to be 1.45 in the frontal cortex [9]. Cerebellum uptake is used as a reference region and is used instead of a plasma input curve. The time–activity curve shows the uptake in the frontal cortex, in the cortex as well as in the cerebellum.

The region-to-cerebellum ratios between 60 and 90 min obtained by μ PET studies ($n=4$) are displayed in Table 2. An improved ratio of 3.3 was found for (R)-[^{18}F]MH.MZ compared to the value of 2.7 for its racemic analogue [^{18}F]MH.MZ. The ratio for the frontal cortex was also improved to be 3.9. According to the time–activity curves (TAC) displayed in Fig. 8, steady state appears to be reached between 28 and 35 min postinjection and the specific binding remains very constant over 60 min. This is identical with that observed with [^{18}F]MH.MZ.

In comparison, [^{11}C]MDL 100907 region-to-cerebellum ratios were shown to be slightly lower compared to those of (R)-[^{18}F]MH.MZ (Table 2) [18]. Therefore, the enantioselective derivative (R)-[^{18}F]MH.MZ is probably the more valuable tracer for molecular imaging of the 5-HT_{2A} receptor system by PET at least in rats.

These observations demonstrate the superior μ PET behavior of (R)-[^{18}F]MH.MZ in comparison to [^{18}F]altanserin at least in rats. [^{18}F]Altanserin, the most used PET ligand to image the 5-HT_{2A} receptor status in human, has recently been shown to be a strong substrate of one efflux transporter in rats, namely, P-glycoprotein (P-gp). Ex vivo as well as in vivo studies in rats showed that altanserin has a limited brain uptake in rats. Consequently, its binding potential (BP) is highly variable [19].

Moreover, we studied the in vivo stability profile of (R)-[^{18}F]MH.MZ. For the analysis of preliminary in vivo metabolism of (R)-[^{18}F]MH.MZ in brain and blood, samples

were treated as described [10]. Metabolite and intact tracer were analyzed by radio-TLC ($\text{CHCl}_3/\text{MeOH}$ 5:2). The tracer underwent fast metabolism comparable to its racemic derivative [10]. Only one polar metabolite was found in plasma, and the percentage of unmetabolized fractions was 40%, 35%, 13% and 5% at 5, 10, 30 and 60 min, respectively. In comparison, Scott and Heath [20] investigated the in vivo metabolism of MDL 100907 and its main metabolite MDL 105725. These pharmacokinetic studies demonstrated that MDL 100907 undergoes a rapid first-pass metabolism [20]. This is very similar to our observed results. Radio-TLC analyses showed nonmetabolized (R)-[^{18}F]MH.MZ within the brain at 60 min postinjection and almost no radioactive metabolite within the brain, as already observed for the racemate [10]. These findings could also be observed for MDL 100907 by Scott and Heath [20]. MDL 100907 as MH.MZ does not appear to be metabolized within the brain [10,20].

In summary, maintained data for (R)-[^{18}F]MH.MZ are in accordance with those of [^{18}F]MH.MZ and MDL 100907 [20].

4. Conclusion

Two new 5-HT_{2A} affine tracers, [^{18}F]DD-1 ($K_i=3.23$ nM) and (R)-[^{18}F]MH.MZ ($K_i=0.72$ nM), were ^{18}F -fluoroalkylated by the secondary synthon [^{18}F]FETos in radiochemical yields of >70%. The final formulation of the injectable solution including [^{18}F]FETos synthesis took no longer than 100 min for the two compounds. The overall RCY was about 40%. It provided ^{18}F -labeled compounds with a purity >96% and a typical specific activity of 35–40 GBq/ μmol with a starting radioactivity of ~ 3 GBq of [^{18}F]fluorine.

Autoradiographic images of 5 and 4 showed excellent visualization of the 5-HT_{2A} receptor for (R)-[^{18}F]MH.MZ and less specific binding for [^{18}F]DD-1 in rat brain slices. This is reasonable for (R)-[^{18}F]MH.MZ due to its increased affinity, but unexpected for [^{18}F]DD-1. The reduced binding for [^{18}F]DD-1 may be explained by its decreased affinity compared to (R)-[^{18}F]MH.MZ; nonetheless, it is unexpected when comparing its affinity with the racemic derivative [^{18}F]MH.MZ. In addition, selectivity of [^{18}F]DD-1 showed no intense alteration compared to that of MH.MZ. Therefore, the observed properties are most probably due to the increased lipophilicity of [^{18}F]DD-1.

Table 2

Region to cerebellum ratios of (R)-[^{18}F]MH.MZ between 60 and 90 min and [^{11}C]MDL 100907 between 20 and 60 min maintained by μ PET studies in rat brains ($n=4$)

Region	(R)-[^{18}F]MH.MZ	[^{11}C]MDL 100907 ¹⁸
Cortex	3.3 \pm 0.2	–
Frontal cortex	3.9 \pm 0.1	2.9

Competition autoradiography experiments were conducted with the new enantioselective tracer to prove its selective binding characteristics. Cortex-to-cerebellum ratios of (*R*)-[¹⁸F]MH.MZ binding were almost twice as high as compared to [¹⁸F]MH.MZ binding. Equal levels of specific activities were used for these experiments.

Results from μ PET scans of (*R*)-[¹⁸F]MH.MZ hint on significantly improved molecular imaging characteristics compared with those of [¹⁸F]MH.MZ due to the higher 5-HT_{2A} binding of (*R*)-MH.MZ ($K_i=0.72$ nM) compared to MH.MZ ($K_i=3.0$ nM). High uptake could be demonstrated in cortex regions. The binding potential of (*R*)-[¹⁸F]MH.MZ was determined to be 2.2 in the cortex and 2.6 in the frontal cortex ($n=4$), whereas the cortex-to-cerebellum ratio was determined to be 3.3 at steady state in the cortex and 3.9 in the frontal cortex (60–90 min, $n=4$). All values represent an important improvement compared to those obtained with [¹⁸F]MH.MZ [9].

Therefore, the enantioselective derivative (*R*)-[¹⁸F]MH.MZ is probably the more valuable tracer for molecular imaging of the 5-HT_{2A} receptor system by PET.

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